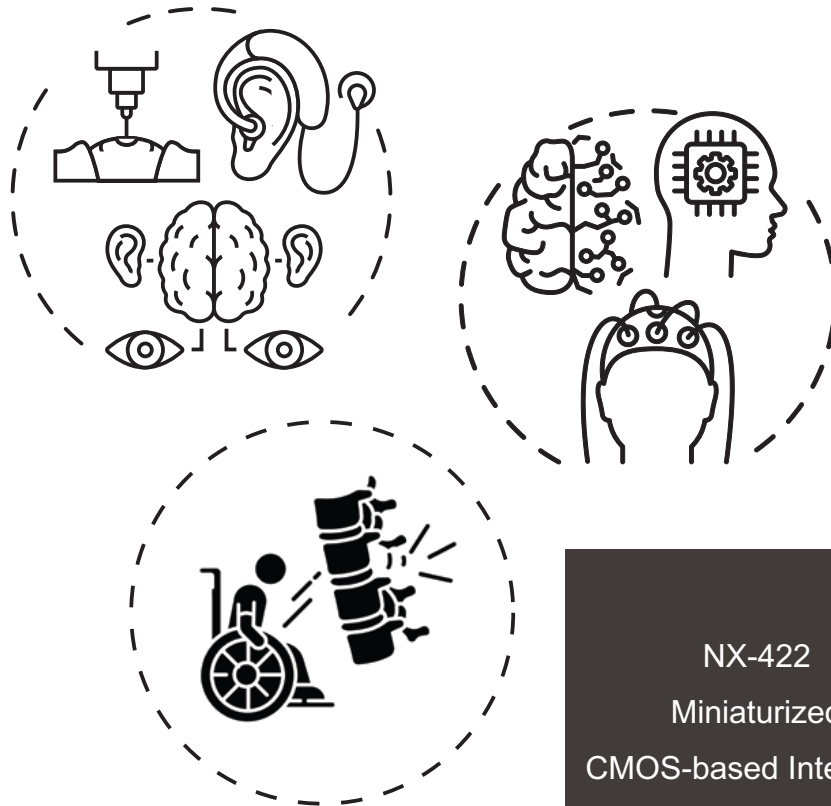
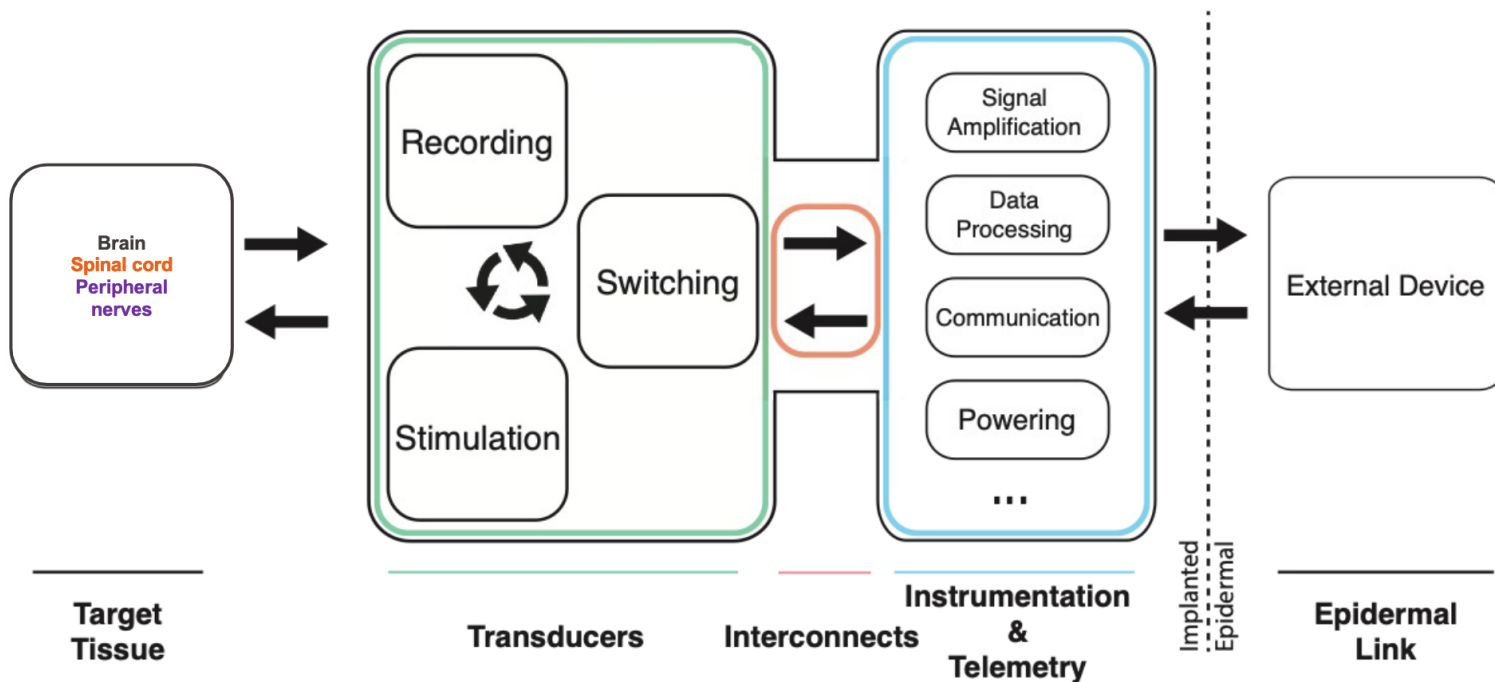




Neural Interfaces

NX-422
Miniaturized
CMOS-based Interfaces

Mahsa Shoaran
IEM and Neuro-X Institutes



- The goal of BCI technology is to give severely paralyzed people alternative ways to communicate

Simple interfaces:

- Paint program, email writing
- TV controls, eating, drinking
- Robotic arm control



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Future:

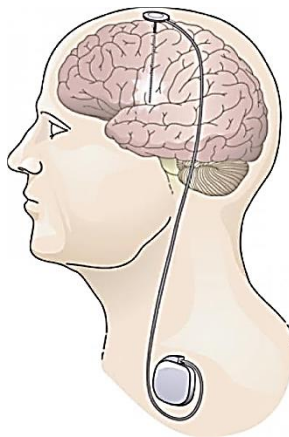
- More electrodes, richer input signal
- Better algorithms and AI for more complex decoding tasks
- **Better hardware for chronic use outside the clinic**



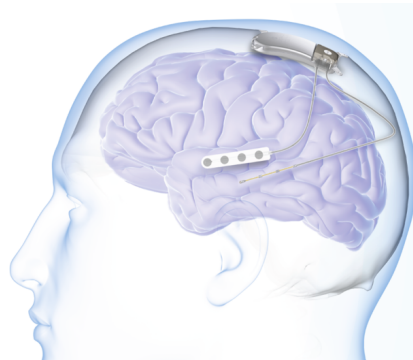
- Neurostimulation to suppress disease symptoms, or replace a function, trigger movement, ...

Future:

- Smaller devices for **minimally-invasive surgery**
- Advanced electronics for **high-resolution recording and safe stimulation**
- Advanced algorithms and circuits for **closed-loop control**

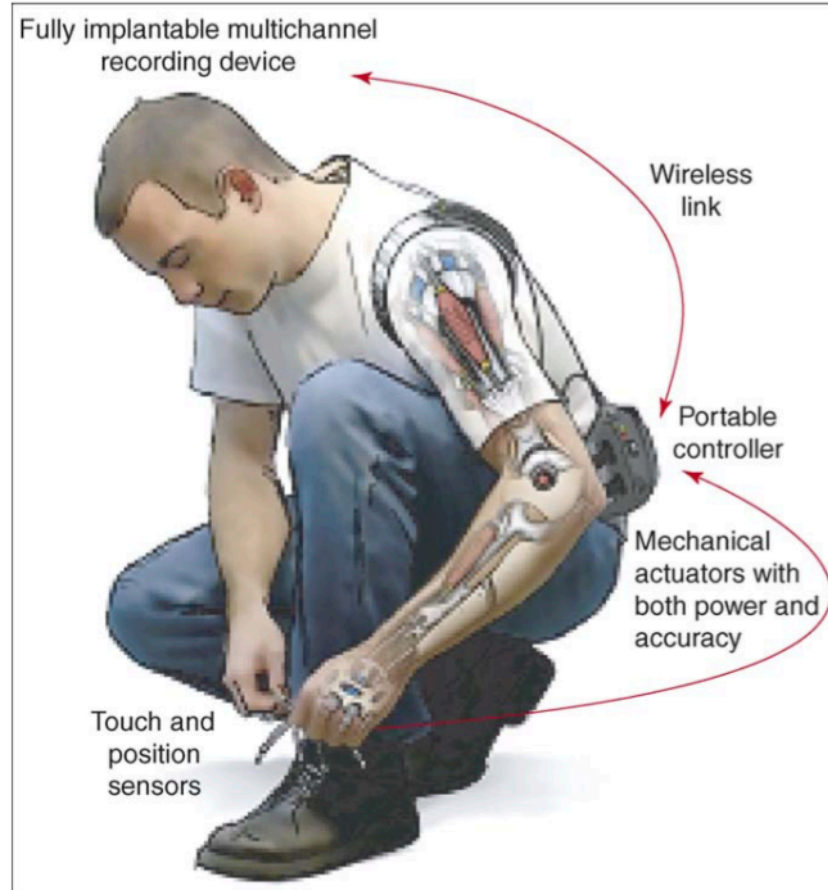


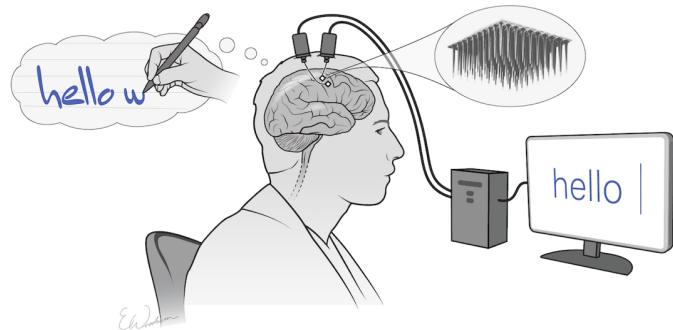
Deep-Brain Stimulation (DBS) for Movement Disorders



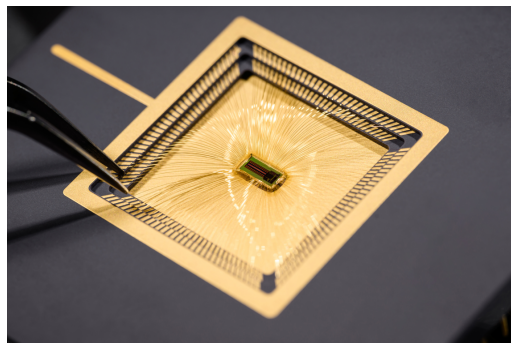
Epilepsy Implants: Seizure Detection and Suppression with Stimulation



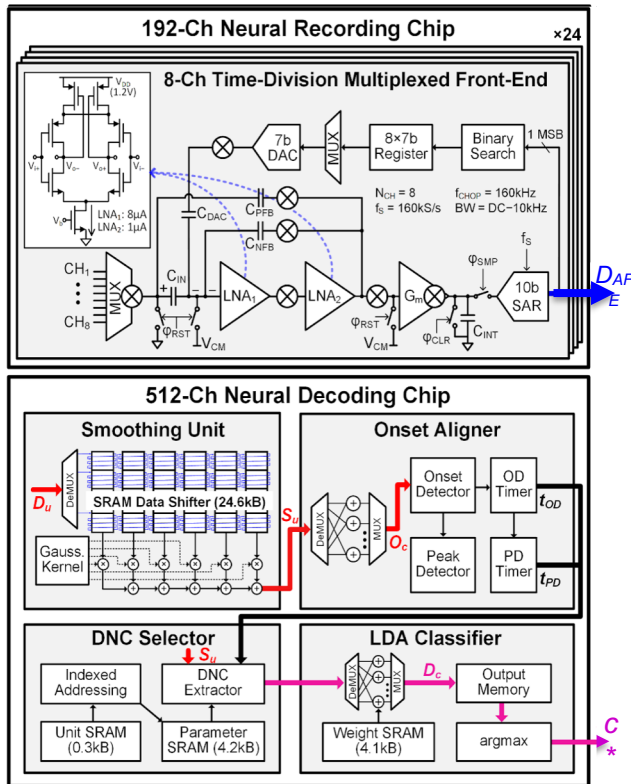




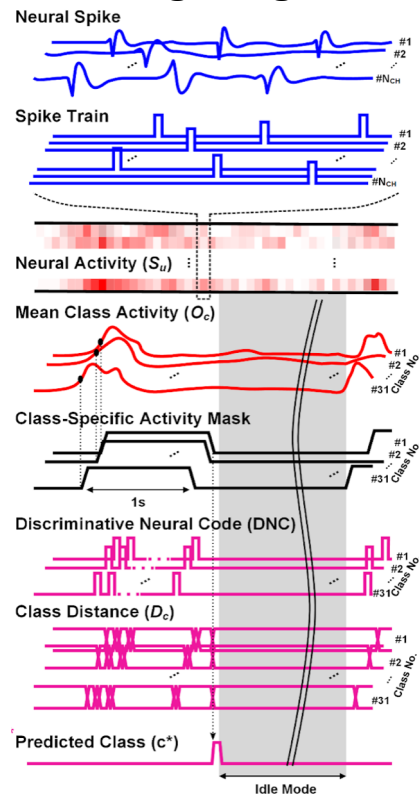
F. R. Willett et al., Nature'21



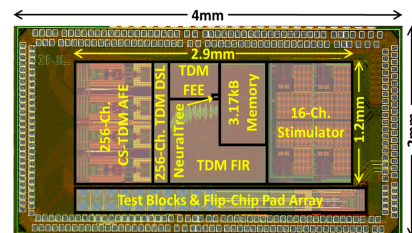
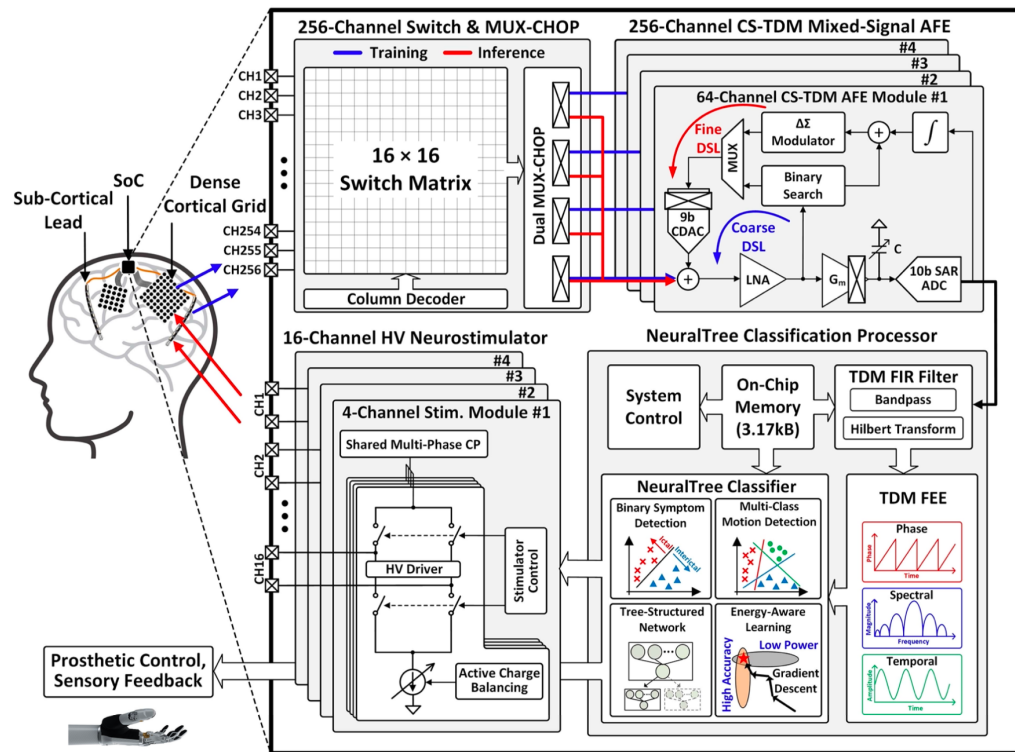
Hardware Architecture



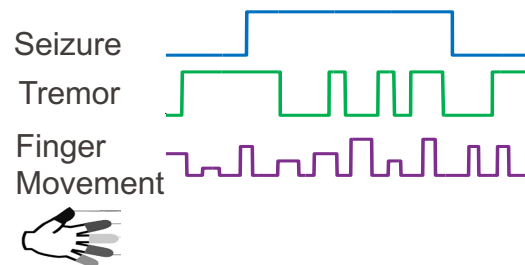
Timing Diagram



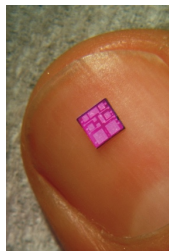
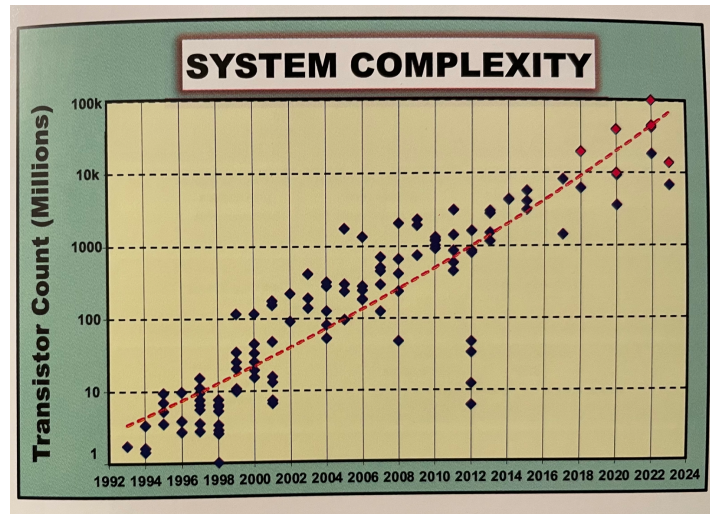
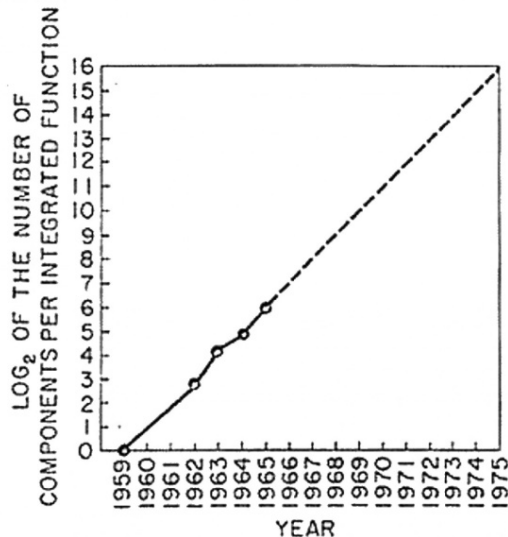
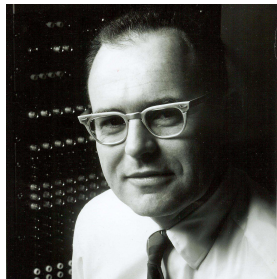
M. Shaeri et al., ISSCC'24, JSSC'24

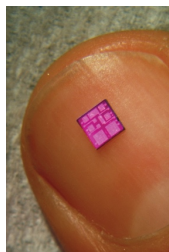
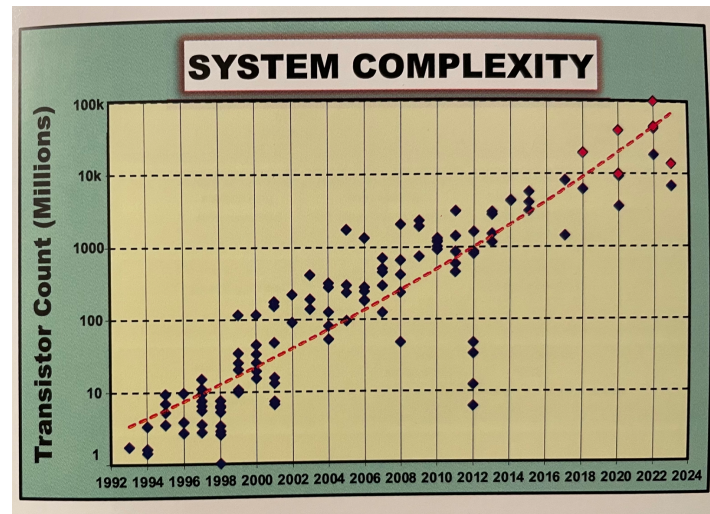
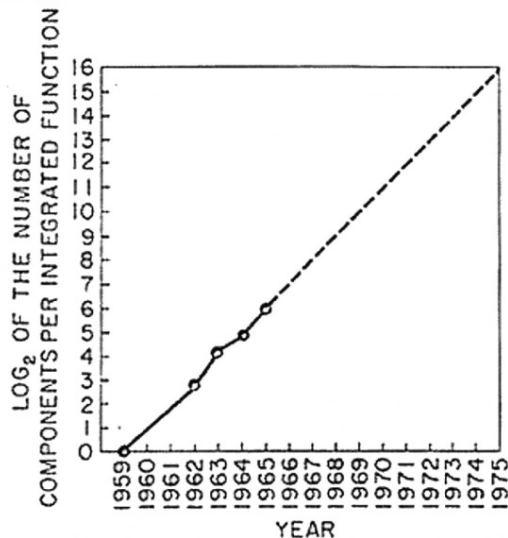
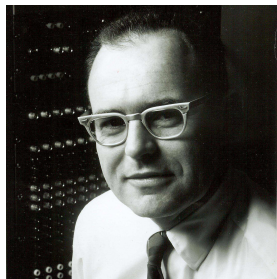
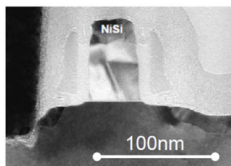
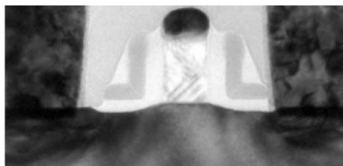
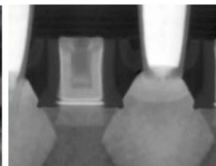
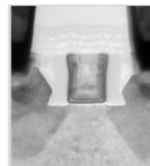


Classifier Output



U. Shin et al., ISSCC'22, JSSC'22

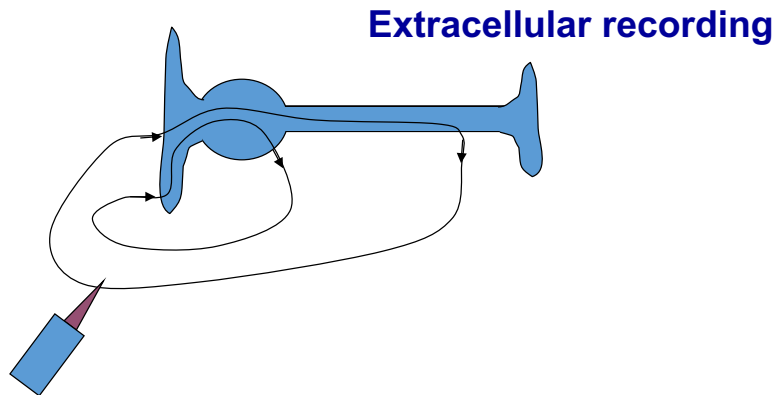


90 nm node65 nm node45 nm node32 nm node

...

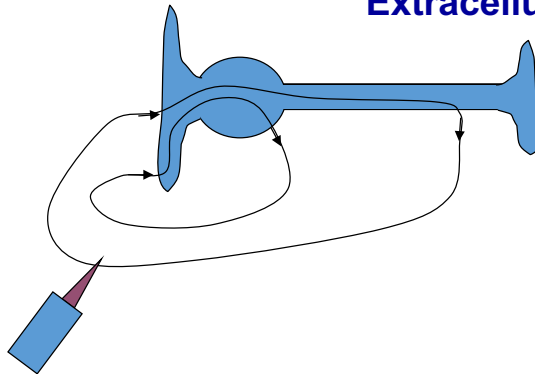
- Types of neural signals, miniaturized implantable systems
- Electrical recording, neural amplifiers
 - low-noise and low-power CMOS design
- Digitization and compression methods and circuits
- Overview of neurostimulation methods and circuits
- Prediction of neurological disorders: hardware implementation
- Closed-loop neuromodulation circuits
- BMI systems

- Two electrodes are placed inside the brain in extracellular medium (one for recording, one for reference)
- During an AP, influx of sodium into cell causes large change in voltage potential in the surrounding area relative to distant areas
- This causes a voltage difference between the recording electrode and the (distant) reference electrode
- We detect small voltages outside, from current looping back to dendrite
- The voltage we detect is much less than the differences in membrane voltage



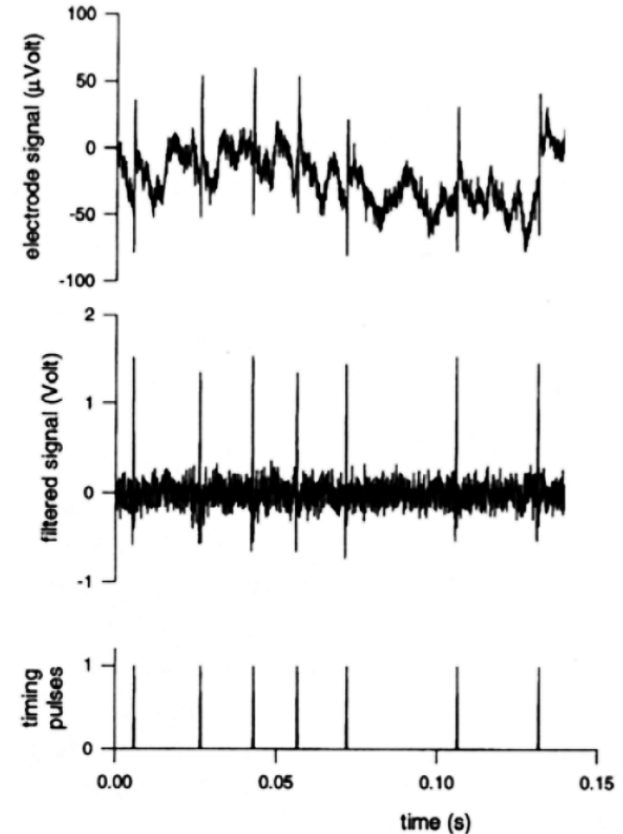
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Extracellular recording



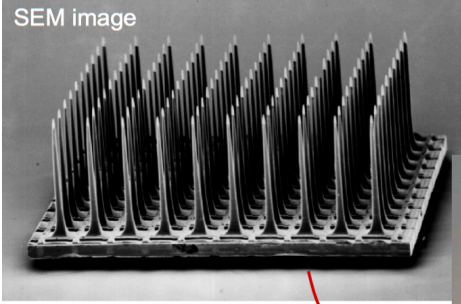
EPFL Extracellular Recording of Action Potentials

- Can only observe action potentials (spikes)
- Assumption: neurons convey information in their spikes
- The rate of spikes carries information

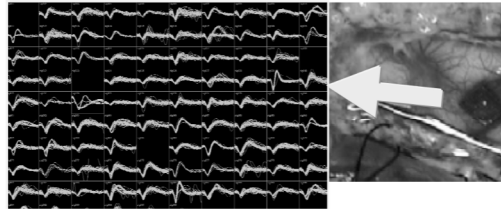
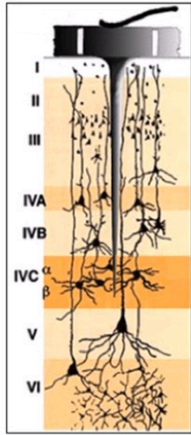
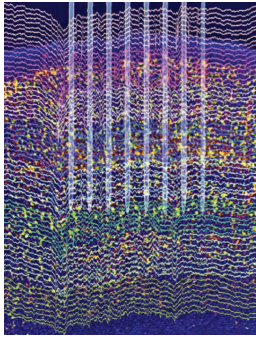
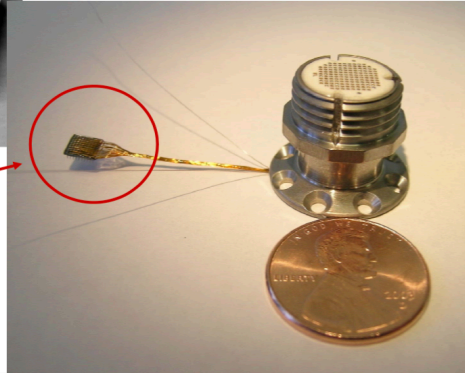


Examples of Extracellular Electrodes

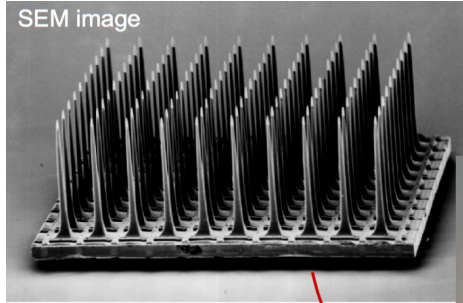
SEM image



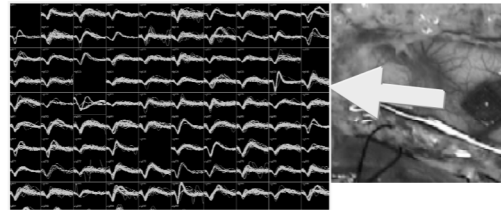
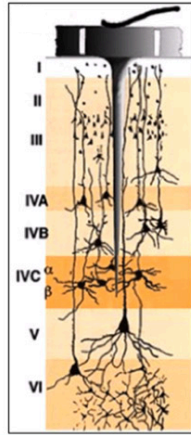
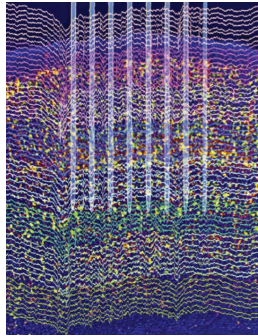
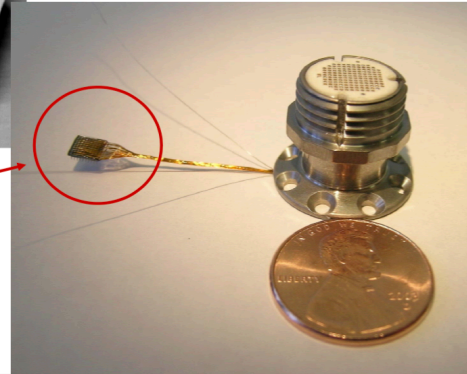
Utah array



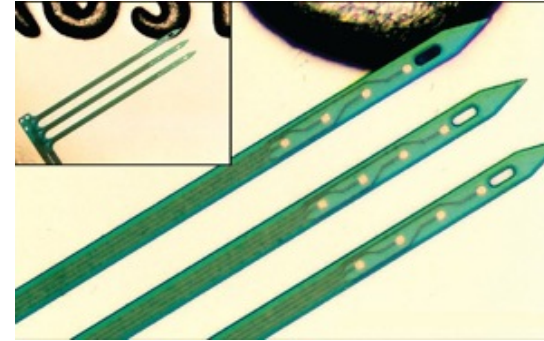
Examples of Extracellular Electrodes



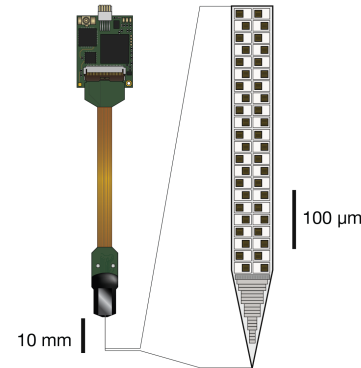
Utah array



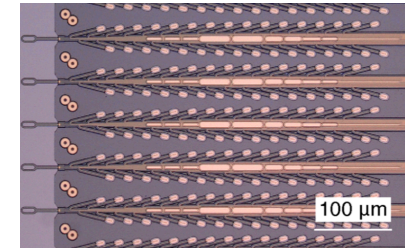
Michigan probes



Neuropixels, 960Ch

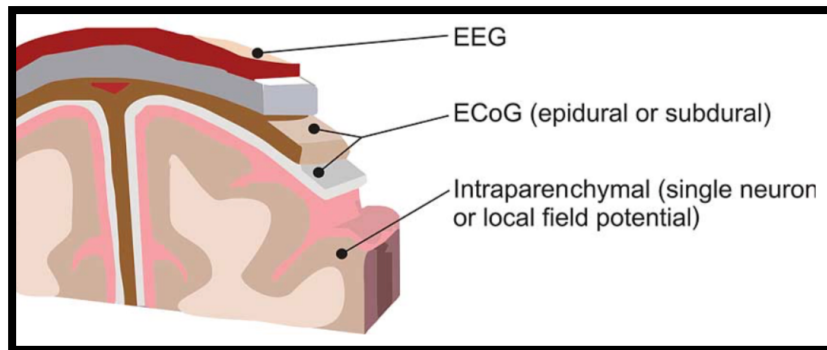
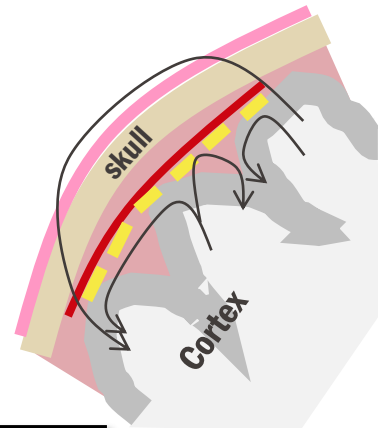
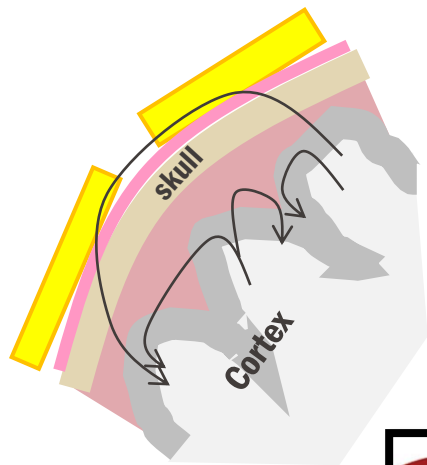


Neural threads, 3072Ch



Neuralink, preprint 2019

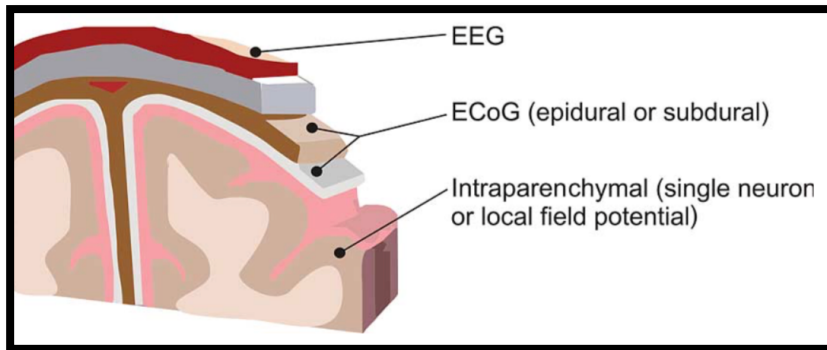
- **EEG**: sheet of electrodes on surface of head (on skin): **not invasive**
- **ECoG**: sheet of electrodes on surface of cortex: **invasive but not brain penetrating**



- **Electrocorticography (ECoG) or intracranial EEG (iEEG)**

Compared to EEG, ECoG has a number of favorable characteristics:

- **Higher spatial resolution** (0.5-10mm versus several centimeters for EEG)
- **Higher amplitude**, easier to capture
- **Less vulnerability to artifacts** such as electromyographic (EMG) or electroocular (EOG) activity
- **Broader bandwidth** (i.e., <500Hz versus <50Hz for EEG)



- < 300 Hz : Local Field Potentials (LFP)
- 300 – 10kHz : Single-Unit Activity (AP or “spikes”)
- Local Field Potential (LFP) – electrical activity of all cells **averaged over some spatial neighborhood**
- **High-pass filtering** in < 1 ms range gives **spikes**
- **LFP signal is lower frequency**

